

# Package: oro.pet (via r-universe)

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**Title** Rigorous - Positron Emission Tomography

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**Description** Image analysis techniques for positron emission tomography (PET) that form part of the Rigorous Analytics bundle.

**Depends** R (>= 2.14.0)

**Imports** methods, oro.dicom (>= 0.4.0), oro.nifti (>= 0.4.0), utils, minpack.lm, msm

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**URL** <http://rig.oro.us.com>, <http://rigorousanalytics.blogspot.com>

**RoxygenNote** 7.2.1

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**Repository** <https://bjw34032.r-universe.dev>

**RemoteUrl** <https://github.com/bjw34032/oro.pet>

**RemoteRef** HEAD

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<code>.petWrapper</code>	<i>Wrapper for oro.pet functions</i>
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**Description**

Simple wrapper for getting functions from

**Usage**

```
.petWrapper(name, ...)
```

**Arguments**

name	name of function (without leading ".")
...	Additional arguments passed to <code>oro.nifti::.wrapper</code>

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<code>activityConcentration</code>	<i>Calculating SUVs for PET Using QIBA Pseudocode</i>
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**Description**

The standard uptake value (SUV) is calculated based on an 18F-FDG-PET acquisition using ancillary information contained in the DICOM data.

**Usage**

```
activityConcentration(pixelData, ...)
```

```
## S4 method for signature 'array'
activityConcentration(
  pixelData,
  CSV = NULL,
  seriesNumber = NULL,
  method = "qiba"
)
```

```
.activityConcentration(
  pixelData,
  CSV = NULL,
  seriesNumber = NULL,
  method = "qiba"
)
```

```
standardUptakeValue(pixelData, ...)
```

```

## S4 method for signature 'array'
standardUptakeValue(
  pixelData,
  mask = NULL,
  CSV = NULL,
  seriesNumber = NULL,
  method = c("qiba", "user"),
  prior = NULL,
  decayedDose = NULL
)

.standardUptakeValue(
  pixelData,
  mask = NULL,
  CSV = NULL,
  seriesNumber = NULL,
  method = c("qiba", "user"),
  prior = NULL,
  decayedDose = NULL
)

```

### Arguments

<code>pixelData</code>	is a multidimensional array of signal intensities of class <code>nifti</code> .
<code>...</code>	additional arguments
<code>CSV</code>	is a <code>data.frame</code> that is the output from <code>dicomTable</code> and contains all necessary DICOM header fields.
<code>seriesNumber</code>	is the <code>SeriesNumber</code> that corresponds to the PET acquisition.
<code>method</code>	takes on two possible values ( <code>qiba</code> and <code>user</code> ), where QIBA pseudocode is used to calculate the SUVs or user-defined parameters are used.
<code>mask</code>	is a multidimensional array of logical values (only used when <code>method = "user"</code> ).
<code>prior</code>	is a list of DICOM header field names that are necessary for the SUV calculation under <code>method = "user"</code> or may be used to replace values from the DICOM header information when <code>method = "qiba"</code> .
<code>decayedDose</code>	is the amount of the <code>RadionuclideTotalDose</code> after being corrected for residual dose in the syringe. This value is NOT usually corrected in the DICOM data.

### Value

A list containing the following items

- `SUVbwis` a multidimensional array, the same dimension as `pixelData`, that contains the standard uptake values.
- `hdris` a list of DICOM header fields used in the SUV calculation.
- `decayTimeis` the decay time calculated from the DICOM header information.

- decayedDose is the RadionuclideTotalDose, if taken from the DICOM header information, or the user-specified value.
- SUVbwScaleFactor is PatientsWeight · 1000/decayedDose.

### Note

Note, for GE scanners it is common for the RescaleSlope DICOM field to vary on a slice-by-slice basis. This is taken into account if a GE scanner is detected from the Modality DICOM field. However, the InstanceNumber is used to reorder the slices so they match the incoming NIfTI file of PixelData. If this is not correct it may be necessary to manually re-order the RescaleSlope field in the CSV data frame so that the activity concentration is calculated correctly.

### Author(s)

Brandon Whitcher <bwhitcher@gmail.com>

### References

[https://qibawiki.rsn.org/index.php?title=Standardized\\_Uptake\\_Value\\_\(SUV\)](https://qibawiki.rsn.org/index.php?title=Standardized_Uptake_Value_(SUV))

### See Also

[dicomTable](#), [nifti](#)

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compartmentalModel      *Compartmental Models for Kinetic Parameter Estimation*

---

### Description

A selection of parametric models are provided that combine a compartmental model for tissue and empirical versions of the arterial input function or reference region time activity curve.

### Usage

```
compartmentalModel(type)
```

### Arguments

type            is a character string that identifies the type of compartmental model to be used. Acceptable models include:

**list("srtm")** Simplified Reference Tissue Model

**list("srtm2")** Simplified Reference Tissue Model in two steps

### Details

Parametric models from the PET literature are provided to the user for kinetic parameter estimation.

**Value**

A function.

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

**References**

Lammertsma, A.A and Hume, S.P. (1996) Simplified reference tissue model for PET receptor studies, *NeuroImage*, **4**, 153-158.

Wu, Y and Carson, R.E. (2002) Noise reduction in the simplified reference tissue model for neuroreceptor functional imaging, *Journal of Cerebral Blood Flow & Metabolism*, **22**, 1440-1452.

**See Also**

[simplifiedReferenceTissueModel](#)

---

expConv

*Empirical Convolution Between an Input Function and a Single Exponential*

---

**Description**

Computationally efficient method to convolve a vector of observations and a single exponential function with two parameters.

**Usage**

```
expConv(input, k1, k2)
```

**Arguments**

input	is the so-called input function.
k1	is the scaling parameter in the single exponential function.
k2	is the decay parameters in the single exponential function.

**Details**

Assuming the input function has been sampled (or interpolated) to a high temporal resolutions, say one Hertz, a simple for loop is used to perform the convolution.

**Value**

The vector containing the result from the convolution operation.

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

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`hillEquation`*Estimation of the Half Maximal Inhibitory Concentration*

---

### Description

The half maximal inhibitory concentration (IC50) is a measure of the effectiveness of a compound in inhibiting biological or biochemical function. This quantitative measure indicates how much of a particular drug or other substance (inhibitor) is needed to inhibit a given biological process (or component of a process) by half.

See reference(s).

In this version of the function the maximal occupancy (rmax) is estimated automatically. This should be optional.

### Usage

```
hillEquation(  
  conc,  
  occ,  
  guess = c(1, 100),  
  control = minpack.lm::nls.lm.control()  
)
```

### Arguments

<code>conc</code>	a vector of drug concentrations in plasma (example units are ng/mL).
<code>occ</code>	a vector of PET occupancy values that correspond to the measured drug concentrations in plasma.
<code>guess</code>	a length-two vector of starting values for the nonlinear optimization.
<code>control</code>	is a list of parameters used by <code>nls.lm.control</code> that are set by default, but may be customized by the user.

### Value

List with the following elements

- `IC50` Half maximal inhibitory concentration
- `rmax` Estimated maximal occupancy
- `IC50SE` Approximate standard error for IC50
- `rmaxSE` Approximate standard error for rmax
- `hessian` Hessian matrix from the Levenburg-Marquardt procedure
- `info` Return value from the Levenburg-Marquardt procedure
- `deviance` Deviance from the Levenburg-Marquardt procedure
- `message` Text message from the Levenburg-Marquardt procedure

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

**References**

[Hill Equation IC50](#)

**See Also**

[nls.lm](#)

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 leanBodyMass

*Calculating the Lean Body Mass*


---

**Description**

The lean body mass (LBM) is calculated according to the formula

$$1.1 \cdot \text{weight} - 128 \cdot (\text{weight}/\text{height})^2$$

if male and

$$1.07 \cdot \text{weight} - 148 \cdot (\text{weight}/\text{height})^2$$

if female.

The standard uptake value (SUV) is summarized using the hotspot method or by calculating total volume of the high values.

**Usage**

```
leanBodyMass(height, weight, gender)
```

```
hotSpotSUV(suv, radius = 10, type = "3D")
```

```
totalSUV(suv, mask, z, bg, local = TRUE)
```

**Arguments**

height	is a vector of heights in centimeters.
weight	is a vector of weights in kilograms.
gender	is a character vector (may be of length one) with the value "male" or "female".
suv	is the standard uptake value (SUV).
radius	is the desired hotspot radius (units = voxels).
type	is a character string (acceptable values are 2D or 3D) that determines the dimension of the hot spot (default = 3D).
mask	is a multidimensional array of logical values.
z	is the slice index.
bg	is the estimated background SUV.
local	is a logical value.

**Value**

Vector of lean body mass values in kilograms.

...

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

**References**

Sugawara, Y., K. R. Zasadny, A. W. Neuhoff, R. L. Wahl (1999) Reevaluation of the Standardized Uptake Value for FDG: Variations with Body Weight and Methods for Correction, *Radiology* **213**: 521–525.

**See Also**

[standardUptakeValue](#)

[leanBodyMass](#)

**Examples**

```
library(oro.pet)
n <- 11
h <- seq(200, 150, length=n)
w <- seq(80, 120, length=n)
cbind(h, w, leanBodyMass(h, w, "male"), leanBodyMass(h, w, "female"))
```

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multilinearReferenceTissueModel

*The Multilinear Reference Tissue Model*

---

**Description**

The multilinear reference tissue model (MRTM) estimates the binding potential from an observed time activity curve without the need for arterial sampling. Instead, a second time activity curve must be provided from a suitable reference region where there is negligible binding.

**Usage**

```
multilinearReferenceTissueModel(
  tac,
  ref,
  time,
  tstar,
  MRTM2 = TRUE,
  k2prime = NULL
)
```



**Arguments**

tac	a vector corresponding to the time activity curve from the tissue (in Bq/mL).
ref	a vector corresponding to the time activity curve from the reference region (in Bq/mL).
time	a vector of average frame times (in minutes).
tstar	the time (in minutes) where the linear relationship between the response and covariates may be assumed to be true.
MRTM2	a logical value that selects the three-parameter model (MRTM) or the two-parameter model (MRTM2), where k2prime is fixed.
k2prime	the value of k2prime that has been fixed.

**Details**

See the references.

The numeric integration required to construct the design matrix is performed by interpolating the time activity curves, both for the tissue and reference region, to one-second resolution and then performing the cumsum operation on them.

Given the nonlinear relationship between binding potential and the regression parameters, the `del tamethod` is used to approximate its standard error.

**Value**

BP	Binding potential
BP.error	Approximate standard error of the binding potential
R1	Ratio of the volumes of distribution for the tissue and reference region (assumes a one-tissue model is valid)
R1.error	Approximate standard error for the ratio
k2	Clearance rate constant from the tissue to plasma (assumes a one-tissue model is valid)
k2.error	Approximate standard error for k2
X	Design matrix used in the linear regression
beta	Regression coefficients

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

**References**

- Ichise, M., Ballinger, J.R., Golan, H., Vines, D., Luong, A., Tsai, S. and Kung, H.F. (1996) Non-invasive quantification of dopamine D2 receptors with iodine-123-IBF SPECT, *Journal of Nuclear Medicine*, **37**, 513-520.
- Ichise, M., Liow, J.-S., Lu, J.-Q., Takano, A., Model, K., Toyama, H., Suhara, T., Suzuki, K., Innis, R.B., Carson, R.E. (2003) Linearized reference tissue parametric imaging methods: Application to [<sup>11</sup>C]DASB positron emission tomography studies of the serotonin transporter in human brain, *Journal of Cerebral Blood Flow & Metabolism*, **23**, 1096-1112.

**See Also**

[cumsum](#), [deltamethod](#)

---

occupancy

*Compute Drug Occupancy with Approximate Standard Errors*

---

**Description**

Receptor occupancy is calculated from positron emission tomography (PET) data as the treatment-induced relative change in the concentration of available (not occupied) receptors.

**Usage**

```
occupancy(base, drug, baseSE = NULL, drugSE = NULL, base.drug.corr = 0)
```

**Arguments**

base	is the baseline binding potential (BPND).
drug	is the post-treatment binding potential (BPND).
baseSE	is the standard error for the baseline BPND.
drugSE	is the standard error for the post-treatment BPND.
base.drug.corr	is the user-specified correlation between baseline and post-treatment binding potentials.

**Details**

Occupancy is calculated using the straightforward and well-known formula. If the standard errors for the two binding potentials are provided, then the delta method is used to approximate the standard error for the estimate of occupancy.

**Value**

OCC	is the percent drug occupancy.
SE	is the approximate standard error of the parameter estimate.

**Author(s)**

Brandon Whitcher <bwhitcher@gmail.com>

**References**

Cunningham VJ, Rabiner EA, Slifstein M, Laruelle M (2010). Measuring drug occupancy in the absence of a reference region: the Lassen plot re-visited, *Journal of Cerebral Blood Flow & Metabolism*, **30**, 46-50.

Passchier J, Gee A, Willemsen A, Vaalburg W, van Waarde A (2002). Measuring drug-related receptor occupancy with positron emission tomography, *Methods*, **27**, 278-286.

**See Also**[deltamethod](#)

---

`plotBindingPotential` *Plot Baseline Versus Post-Treatment Binding Potentials*

---

**Description**

Inspired by the Lassen plot (Cunningham et al., 2010) this is a straightforward graphical summary of pre-treatment versus post-treatment binding potentials for a single subject across multiple brain regions.

**Usage**

```
plotBindingPotential(  
  base,  
  drug,  
  lty45 = 2,  
  lty = 1,  
  lwd45 = 2,  
  lwd = 3,  
  col45 = "darkgrey",  
  col = "orange",  
  pch = 1,  
  cex = 1,  
  xlim = range(0, base, 0.5),  
  ylim = range(0, drug, 0.5),  
  xlab = expression(BP[ND]^{  
    Base  
  }),  
  ylab = expression(BP[ND]^{  
    Drug  
  }),  
  ...  
)
```

**Arguments**

<code>base</code>	is the vector of baseline binding potentials across brain regions.
<code>drug</code>	is the vector of post-treatment binding potentials across brain regions.
<code>lty45</code>	is the line type for the 45-degree line.
<code>lty</code>	is the line type for the estimated regression line.
<code>lwd45</code>	is the line width for the 45-degree line.
<code>lwd</code>	is the line width for the estimated regression line.
<code>col45</code>	is the color for the 45-degree line.

col	is the color for the estimated regression line.
pch	is the plotting character symbol.
cex	is the size of the plotting symbol.
xlim	is the range of values on the x-axis.
ylim	is the range of values on the y-axis.
xlab	is the label on the x-axis.
ylab	is the label on the y-axis.
...	additional arguments to be passed to the plot function.

### Details

See the reference below.

### Value

A plot is shown, NULL is returned

### Author(s)

Brandon Whitcher <bwhitcher@gmail.com>

### References

Cunningham VJ, Rabiner EA, Slifstein M, Laruelle M (2010). Measuring drug occupancy in the absence of a reference region: the Lassen plot re-visited, *Journal of Cerebral Blood Flow & Metabolism*, **30**, 46-50.

### See Also

[par](#), [plot](#)

---

simplifiedReferenceTissueModel

*The Simplified Reference Tissue Model*

---

### Description

The simplified reference tissue model (SRTM) estimates the binding potential from an observed time activity curve without the need for arterial sampling. It assumes a one-tissue compartment model to describe the influx and efflux in the tissue region of interest and the reference region.

**Usage**

```
simplifiedReferenceTissueModel(
  tac,
  ref,
  time,
  SRTM2 = TRUE,
  k2prime = NULL,
  guess = c(R1 = 0.5, k2 = 0.01),
  control = minpack.lm::nls.lm.control()
)
```

**Arguments**

<code>tac</code>	a vector corresponding to the time activity curve from the tissue (in Bq/mL).
<code>ref</code>	a vector corresponding to the time activity curve from the reference region (in Bq/mL).
<code>time</code>	a vector of average frame times (in minutes).
<code>SRTM2</code>	a logical value that selects the three-parameter model (SRTM) or the two-parameter model (SRTM2), where <code>k2prime</code> is fixed.
<code>k2prime</code>	the value of <code>k2prime</code> that has been fixed.
<code>guess</code>	values for the initial parameter estimates for <code>R1</code> and <code>k2</code> .
<code>control</code>	a list of parameters used by <code>nls.lm.control</code> that are set by default, but may be customized by the user.

**Details**

See the references.

The model has been parameterized in the manner of Wu and Carson (2002). That is, the nonlinear regression estimates `R1`, `k2` and `k'2` for the three-parameter model (SRTM) and `R1` and `k2` for the two-parameter model (SRTM2).

The convolution is performed after interpolating the time activity curves, both for the tissue and the reference region, to one-second resolution then downsampling them back to the original sampling rate.

**Value**

<code>BP</code>	Binding potential
<code>R1</code>	Ratio of the volumes of distribution for the tissue and reference region
<code>k2</code>	Clearance rate constant from the tissue to plasma
<code>BP.error</code>	Approximate standard error of the binding potential
<code>R1.error</code>	Approximate standard error for the ratio
<code>k2.error</code>	Approximate standard error for <code>k2</code>

**Author(s)**

Brandon Whitcher <b.whitcher@gmail.com>

**References**

Lammertsma, A.A. and Hume, S.P. (1996) Simplified reference tissue model for PET receptor studies, *NeuroImage*, **4**, 153-158.

Wu, Y. and Carson, R.E. (2002) Noise reduction in the simplified reference tissue model for neuroreceptor functional imaging, *Journal of Cerebral Blood Flow & Metabolism*, **22**, 1440-1452.

**See Also**

[deltamethod](#), [expConv](#), [nls.lm](#)

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